



Optical spectroscopy and biosensors for investigation of biomolecules and their interactions

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Tutorial 2: Evaluation of SPR Binding Kinetics for Affinity Interaction Analysis

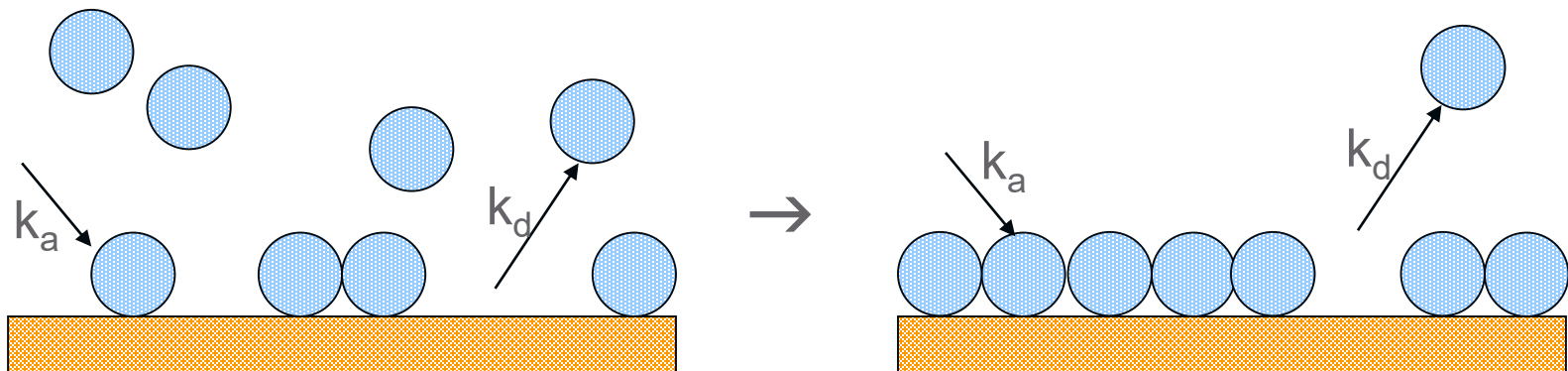


Content

- **Mass transfer and affinity – driven molecular binding kinetics.**
- **Design of the experiment to suppress the impact of diffusion limited binding kinetics.**
- **Tutorial on the fitting of equilibrium sensor response, fitting of the kinetics that are affinity driven, global analysis and taking into account the mass transfer.**

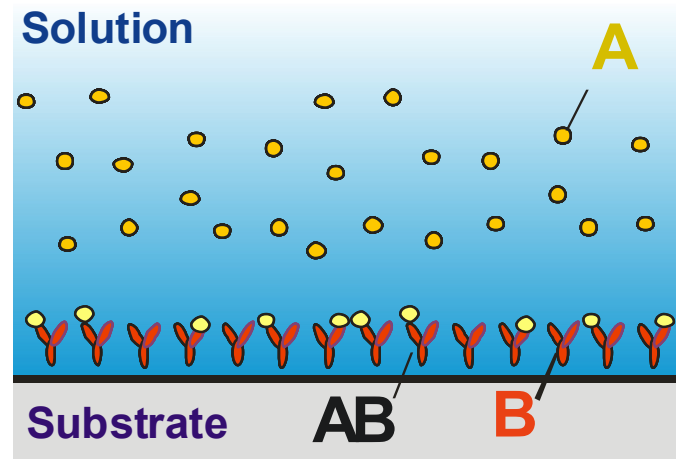
Langmuir Adsorption Isotherm: Assumptions

- All adsorption sites identical
- Adsorbed species interact only with adsorption sites, not with each other
- Adsorption limited to a monolayer



Langmuir Adsorption Isotherm

Equilibrium of a reaction:



Kinetics of the reaction
on a surface:

$$\frac{d\gamma}{dt} = k_a \alpha_0 (\beta - \gamma) - k_d \gamma$$

γ Concentration of [AB]

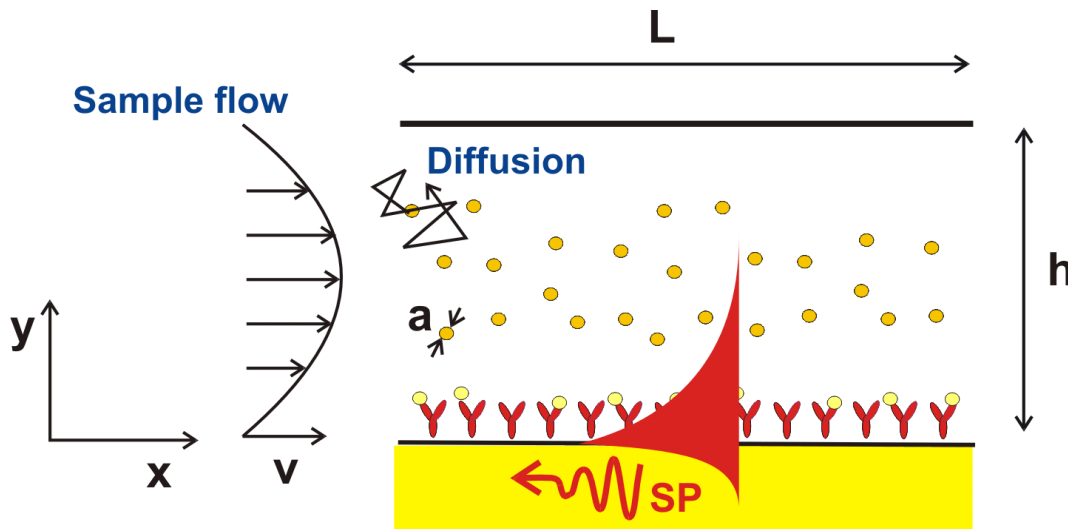
α_0 Concentration [A]

β Concentration [B]

Describes the interaction for:

- Identical monovalent receptors B
 - Constant concentration of A in the solution ($[A] \gg [B]$)
- (Possible to describe more complicated interactions e.g. multivalent receptors)

Two Compartment Model



D – diffusion coefficient

$$D \approx \frac{k_B T}{6\pi a \eta}$$

a – molecule A hydrodynamic radius

η - solution viscosity

In SPR biosensors, analyte molecules A in a liquid samples are flowed over the sensor surface.

Due to the friction, at the surface the flow velocity is $v=0$. Approximation that the analyte mass transfer rate occurs across an unstirred layer through diffusion:

$$k_m = \xi \left(\frac{v_{\max} D^2}{hL} \right)^{1/3}$$

Full Model

A) Description of laminar flow and diffusion in a flow-cell

$$\frac{\partial \alpha(x, y, t)}{\partial t} = D \left(\frac{\partial^2 \alpha(x, y, t)}{\partial^2 x} + \frac{\partial^2 \alpha(x, y, t)}{\partial^2 y} \right) - 4v_{\max} \frac{y}{h} \left(1 - \frac{y}{h} \right) \frac{\partial \alpha(x, y, t)}{\partial x}$$

B) Binding to receptors on the flow-cell bottom

$$\frac{\partial \gamma(x, t)}{\partial t} = k_a \alpha(x, 0, t) [\beta - \gamma(x, t)] - k_d \gamma(x, t)$$

C) Boundary conditions :

$$D \frac{\partial \alpha(x, h, t)}{\partial y} = 0 \quad D \frac{\partial \alpha(x, 0, t)}{\partial y} = \frac{\partial \gamma(x, t)}{\partial t}$$

Mass Transport Limited Kinetics

„Corrected Langmuir equation“:

Valid when the diffusion parallel
 the sensor surface can be omitted
 (diffusion is much slower than
 the flow through the flow-cell)

$$Pe = \frac{v_{\max} h^2}{DL} \gg 1$$

Mass transport can be omitted
 when Damköhler number $Da \ll 1$:

$$Da = k_a \beta \left(\frac{v_{\max} D^2}{hL} \right)^{-1/3} \ll 1 \quad \longrightarrow \quad k_a^{\text{eff}} \approx k_a \quad k_d^{\text{eff}} \approx k_d$$

$$\frac{d\langle \gamma \rangle}{dt} = k_a^{\text{eff}} \alpha_0 (\beta - \langle \gamma \rangle) - k_d^{\text{eff}} \langle \gamma \rangle$$

$$k_a^{\text{eff}} = \frac{k_a}{1 + k_a [\beta - \langle \gamma \rangle(t)] / k_M}$$

$$k_d^{\text{eff}} = \frac{k_d}{1 + k_a [\beta - \langle \gamma \rangle(t)] / k_M}$$

$$k_M \approx 1.378 \left(\frac{v_{\max} D^2}{hL} \right)^{1/3}$$

Surface Reaction with Mass Transfer

Reaction kinetics become a function of mass transfer rate k_m .

$$\frac{d\gamma}{dt} = k_{on}\alpha(\beta - \gamma) - k_{off}\gamma$$

$$k_{on} = \frac{k_a}{1 + k_a \left[\beta - \gamma(t) \right] / k_m}$$

$$k_{off} = \frac{k_d}{1 + k_a \left[\beta - \gamma(t) \right] / k_m}$$

Fast diffusion

$$k_m \gg k_a\beta$$

Reaction is affinity-controlled
and $k_{on} \approx k_a$, $k_{off} \approx k_d$

Slow diffusion

$$k_m \ll k_a\beta$$

Reaction is diffusion-controlled,
 $k_{on} \approx k_m\beta^{-1}$ and
 $k_{off} \approx k_mk_d(k_a\beta)^{-1}$

(low probe / ligand density, high flow rate)



Typical Characteristics

Properties of biomolecules:

Affinity constants: $k_a=10^3-10^7 \text{ M}^{-1}\text{s}^{-1}$ and $k_d=10^{-4}-0.1 \text{ s}^{-1}$ for majority of protein-protein interactions.

Diffusion constant: $D=2.4 \times 10^{-7} \text{ cm}^2\text{s}^{-1}$ for water, $T=20 \text{ }^\circ\text{C}$ and a molecule with the diameter $a=10 \text{ nm}$.

Fluidic system parameters:

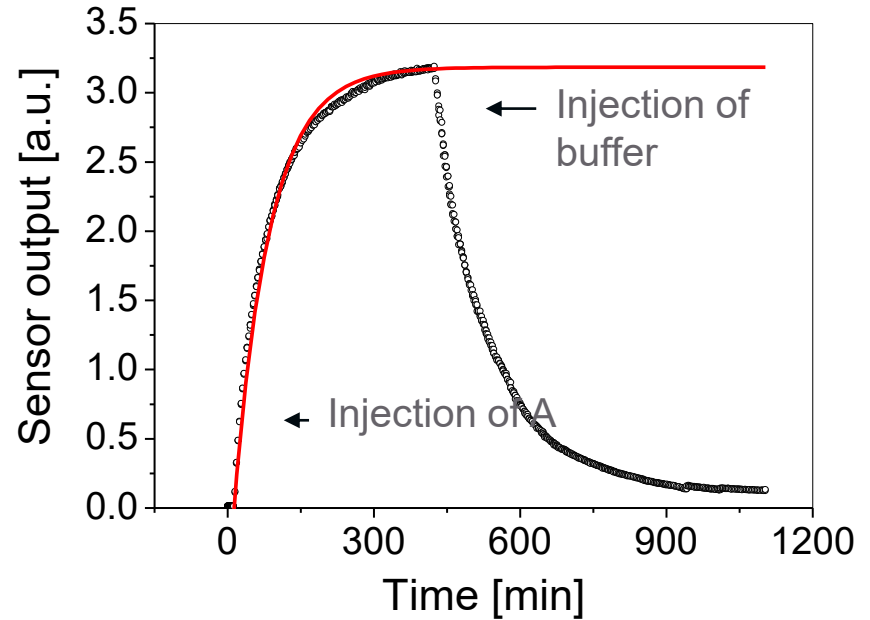
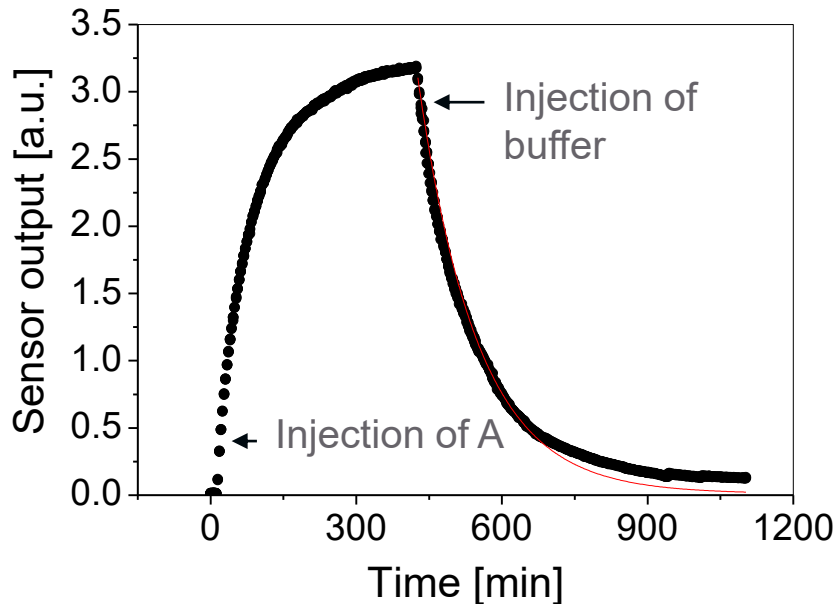
Flow-rate: $\theta=100 \text{ }\mu\text{L}/\text{min}$

Flow-cell parameters: width $w=5\text{mm}$, height $h=0.5\text{mm}$, length
 $L=10\text{mm}$

Peculé number: $Pe\sim 400$ ($\gg 1$ needed)

Damköhler number: $Da\sim 10^{-3}$ ($\ll 1$ needed) for $\beta=10 \text{ ng mm}^2$, $MW=160 \text{ kDa}$,
 $k_a=10^7 \text{ M}^{-1}\text{s}^{-1}$, $D=2.4 \times 10^{-5} \text{ mm}^2\text{s}^{-1}$, $h=0.5 \text{ mm}$, $Pe=400$

Fitting of the Sensor Kinetics

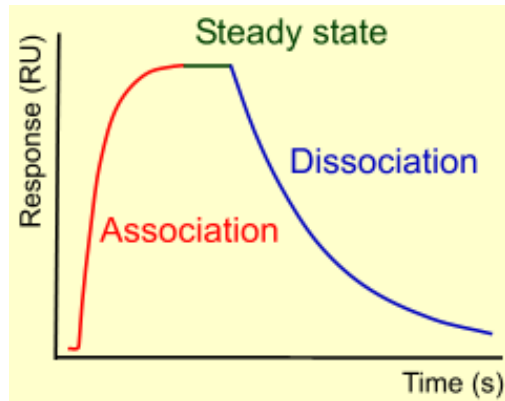


SPR biosensor output $R(t)$ is proportional to $\gamma(t)$, one can fit k_a and k_d as:

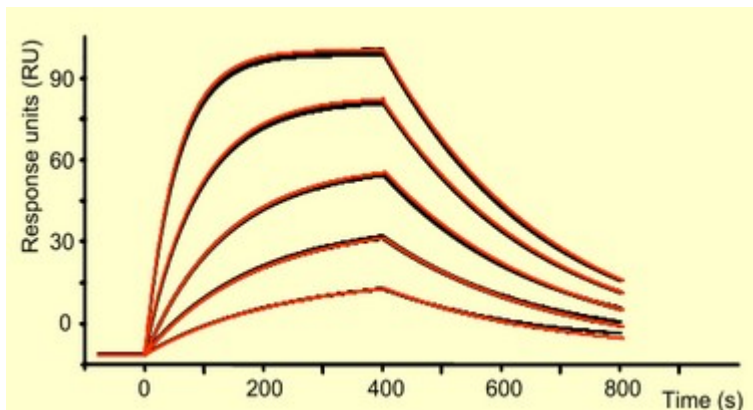
$$R_d(t) = (R_{\max} - R_0) e^{-k_d(t-t_a)} + R_0 \quad R_a(t) = (R_{\max} - R_0) (1 - e^{-(k_a c_0 - k_d)(t-t_0)}) + R_0$$

\downarrow
 $k_d!$
 \downarrow
 $k_a!$

Global Analysis



Fitting kinetics



- ➔ Association and dissociation binding rates (k_a and k_d , respectively) or more complex parameters can be determined by fitting with a model.
- ➔ Analysis can be performed through specialized software (e.g. from BIAcore, Scrubber) or by another tools allowing fitting with non-linear functions (e.g. Origin).

